

Dynamic Regulation of Fibrinogen: Integrin  $\alpha$ IIB $\beta$ 3 Binding<sup>†</sup>Roy R. Hantgan,<sup>\*,‡</sup> Mary C. Stahle,<sup>‡</sup> and Susan T. Lord<sup>§</sup><sup>‡</sup>Department of Biochemistry, Wake Forest University School of Medicine, Medical Center Boulevard, Winston-Salem, North Carolina 27157-1016, and <sup>§</sup>Department of Pathology and Laboratory Medicine, University of North Carolina, Chapel Hill, North Carolina 27599

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**ABSTRACT:** This study demonstrates that two orthogonal events regulate integrin  $\alpha$ IIB $\beta$ 3's interactions with fibrinogen, its primary physiological ligand: (1) conformational changes at the  $\alpha$ IIB– $\beta$ 3 interface and (2) flexibility in the carboxy terminus of fibrinogen's  $\gamma$ -module. The first postulate was tested by capturing  $\alpha$ IIB $\beta$ 3 on a biosensor and measuring binding by surface plasmon resonance. Binding of fibrinogen to eptifibatide-primed  $\alpha$ IIB $\beta$ 3 was characterized by a  $k_{\text{on}}$  of  $\sim 2 \times 10^4 \text{ L mol}^{-1} \text{ s}^{-1}$  and a  $k_{\text{off}}$  of  $\sim 8 \times 10^{-5} \text{ s}^{-1}$  at 37 °C. In contrast, even at 150 nM fibrinogen, no binding was detected with resting  $\alpha$ IIB $\beta$ 3. Eptifibatide competitively inhibited fibrinogen's interactions with primed  $\alpha$ IIB $\beta$ 3 ( $K_i \sim 0.4 \text{ nM}$ ), while a synthetic  $\gamma$ -module peptide (HHLGGAKQAGDV) was only weakly inhibitory ( $K_i > 10 \mu\text{M}$ ). The second postulate was tested by measuring  $\alpha$ IIB $\beta$ 3's interactions with recombinant fibrinogen, both normal (rFgn) and a deletion mutant lacking the  $\gamma$ -chain AGDV sites (rFgn  $\gamma\Delta 408$ –411). Normal rFgn bound rapidly, tightly, and specifically to primed  $\alpha$ IIB $\beta$ 3; no interaction was detected with rFgn  $\gamma\Delta 408$ –411. Equilibrium and transition-state thermodynamic data indicated that binding of fibrinogen to primed  $\alpha$ IIB $\beta$ 3, while enthalpy-favorable, must overcome an entropy-dominated activation energy barrier. The hypothesis that fibrinogen binding is enthalpy-driven fits with structural data showing that its  $\gamma$ -C peptide and eptifibatide exhibit comparable electrostatic contacts with  $\alpha$ IIB $\beta$ 3's ectodomain. The concept that fibrinogen's  $\alpha$ IIB $\beta$ 3 targeting sequence is intrinsically disordered may explain the entropy penalty that limits its binding rate. In the hemostatic milieu, platelet–platelet interactions may be localized to vascular injury sites because integrins must be activated before they can bind their most abundant ligand.

Regulated fibrinogen binding to some 80000  $\alpha$ IIB $\beta$ 3 integrins resident on human blood platelets is essential to normal hemostasis and aberrant in thrombosis (1, 2). Despite their crucial role in human health and disease, defining the molecular mechanisms that shift  $\alpha$ IIB $\beta$ 3 from a quiescent heterodimer to a hemostatically active receptor remains a challenge (3–6). Recent evidence indicates that intracellular integrin activation involves talin binding to the  $\beta$ 3 cytodomain, triggering subunit shifts that ultimately extend the ectodomain (7, 8). Advances in structural biology also support outside-in signaling models in which subtle conformational changes linked to ligand binding at the  $\alpha$ IIB  $\beta$ -propeller– $\beta$ 3 I domain interface (6, 9, 10) are allosterically coupled to rearrangements of the receptor's transmembrane segments and cytodomains (11–14). Pharmaceutical integrin ligands present a twist: they bind to resting  $\alpha$ IIB $\beta$ 3, but it then populates an active form that persists for hours after their dissociation (15, 16).

While platelet stimulation is clearly prerequisite for fibrinogen binding, affinity estimates ( $K_d$ ) for this abundant protein (plasma concentration of  $\sim 10 \mu\text{M}$ ) range from  $< 100 \text{ nM}$  (17–19) to  $> 2 \mu\text{M}$  (20, 21). Studies incorporating  $\alpha$ IIB $\beta$ 3 in lipid vesicles yielded  $K_d$  values from 5 to 15 nM (22–24), but uncertainty about the

receptors' activation state raises new questions. Subsequent reports using solid-phase binding assays indicated that fibrinogen binds rapidly ( $k_{\text{on}} \sim 8 \times 10^5 \text{ L mol}^{-1} \text{ s}^{-1}$ ) (25) and tightly ( $K_d \sim 60 \text{ nM}$ ) (26) to immobilized  $\alpha$ IIB $\beta$ 3. However, those affinity-purified integrins were isolated by a process that selects for preactivated receptors (27, 28), so binding regulation was not addressed. In contrast, Du et al. (29) demonstrated that  $\alpha$ IIB $\beta$ 3 acquired the ability to bind fibrinogen ( $K_d \sim 50 \text{ nM}$ ) following overnight incubation with, and then washout of, synthetic peptide GRGDSP or HHLGGAKQAGDV,<sup>1</sup> albeit at a large molar excess.

Biophysical studies subsequently revealed multistep fibrinogen binding kinetics and raised new questions. The pioneering surface plasmon resonance (SPR) studies of Huber et al. (30) illustrate a quandary. Their biosensor-immobilized integrins only reproducibly interacted with fibrinogen after several cycles of surface regeneration with an RGD peptide. That fits with our observation that RGD peptides shift the initially resting receptor to an open conformation (31). They reported a rapid initial on rate  $k_{\text{on}}$  of  $\sim 3 \times 10^5 \text{ L mol}^{-1} \text{ s}^{-1}$  and a  $K_d$  of 165 nM (30). Muller et al. (32) described total internal reflection fluorescence measurements with unstimulated  $\alpha$ IIB $\beta$ 3 reconstituted in lipid bilayers. They found a

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<sup>1</sup>Abbreviations: HSCM, pH 7.4 buffer containing 0.13 mol/L NaCl, 0.01 mol/L HEPES, 0.001 mol/L  $\text{CaCl}_2$  and 0.001 mol/L  $\text{MgCl}_2$ ; HSCM-OG, HSCM buffer with 0.03 mol/L *n*-octyl- $\beta$ -D-glucopyranoside; HSCM-T, HSCM buffer with 0.01% Tween; RU, response units; SPR, surface plasmon resonance; HHLGGAKQAGDV, synthetic peptide L-histidyl-L-histidyl-L-leucyl-glycyl-glycyl-L-alanyl-L-lysyl-L-glutamyl-L-alanyl-glycyl-L-aspartyl-L-valine.

slower  $k_{on}$  of  $\sim 4 \times 10^4 \text{ L mol}^{-1} \text{ s}^{-1}$ , for the initial binding event but a smaller  $K_d$  of  $\sim 50 \text{ nM}$ ; slower formation of an irreversible complex followed. In contrast, Pesho et al. (33) fit their SPR data to a 1:1 binding model for fibrinogen's interactions with RGD-purified  $\alpha\text{IIb}\beta 3$  covalently coupled to biosensors. They obtained a  $k_{on}$  of  $\sim 3 \times 10^5 \text{ L mol}^{-1} \text{ s}^{-1}$  and a much tighter  $K_d$  of  $\sim 3 \text{ nM}$ . To resolve the relationship between integrin activation and the rate or affinity of fibrinogen binding, we purified  $\alpha\text{IIb}\beta 3$  in a resting conformation (34) that can be modulated by transient exposure to a priming ligand prior to delivery of a macromolecule for SPR binding studies (16).

The fibrinogen ( $\text{A}\alpha\text{B}\beta\gamma$ )<sub>2</sub> molecule is rich in potential integrin recognition sites, with classic RGD sequences midway through the  $\alpha$ -chains' coiled-coil regions and on their carboxy-terminal segments. However, fibrinogen molecules with RGE substitutions at A $\alpha$  95–97 or A $\alpha$  572–574 supported aggregation of ADP-stimulated platelets as effectively as plasma fibrinogen (35) or normal recombinant fibrinogen (36). Fibrinogen's  $\gamma$ -chains also have a unique  $\alpha\text{IIb}\beta 3$  targeting sequence, HHLGGAK-QAGDV (37, 38). The plasma fibrinogen variant ( $\text{A}\alpha\text{B}\beta\gamma'$ ) ( $\text{A}\alpha\text{B}\beta\gamma$ ), which lacks that sequence on one of its  $\gamma$ -chains, exhibited only half-maximal activity in platelet aggregation and fibrinogen binding assays (35, 39). Likewise, recombinant ( $\text{A}\alpha\text{B}\beta\gamma'$ )<sub>2</sub> showed a markedly decreased level of platelet binding (40), and a recombinant fibrinogen variant with its  $\gamma$ -chain AGDV sites deleted (rFgn  $\gamma\Delta 408$ –411) failed to support platelet aggregation (36, 41). In contrast, another recombinant fibrinogen variant with dysfunctional  $\alpha$ -chain RGE sites and deleted  $\gamma$ -chain AGDV sites exhibited substantial clot retraction (36). Auxiliary integrin-binding sites localized to  $\gamma 316$ –322 (42–44) and  $\gamma 370$ –381 (45, 46) may play special roles in mediating the adhesion of platelets to immobilized fibrinogen and clotted fibrin.

While these observations strongly suggest that  $\alpha\text{IIb}\beta 3$ –fibrinogen interactions are mediated not by its RGD sites but rather by residues present on its  $\gamma$ -module, this concept has not been rigorously tested in a purified system. Here, we present evidence from SPR measurements performed with recombinant fibrinogen, both normal and rFgn  $\gamma\Delta 408$ –411, that residues on the carboxy terminus of its  $\gamma$ -module are essential for tight binding to primed  $\alpha\text{IIb}\beta 3$ . Combining our equilibrium and transition-state thermodynamic data with structural insights, we propose a new model for the dynamic regulation of integrin–fibrinogen interactions.

## EXPERIMENTAL PROCEDURES

**$\alpha\text{IIb}\beta 3$  Purification.** Milligram quantities of highly purified  $\alpha\text{IIb}\beta 3$  were isolated from outdated human blood platelets (Blood Bank, North Carolina Baptist Hospital, Winston-Salem, NC) by affinity and size-exclusion chromatography in HSCM-OG buffer as previously described (47).

**Anti- $\alpha\text{IIb}$  Cytoplasmic IgG.** Antibody A4 was isolated by affinity chromatography from the serum of rabbits immunized with a synthetic peptide, L-cysteiny-L-prolyl-L-leucyl-L-glutamyl-L-glutamyl-L-aspartyl-L-aspartyl-L-glutamyl-L-glutamyl-glycyl-L-glutamic acid, corresponding to the 10 carboxy-terminal residues of the  $\alpha\text{IIb}$  cytoplasmic domain as previously described (16).

**Integrin Antagonists.** COR Therapeutics (San Francisco, CA) provided eptifibatide [Integrilin;  $N^6$ -(aminoiminomethyl)- $N^2$ -(3-mercapto-1-oxopropyl-L-lysylglycyl-L- $\alpha$ -aspartyl-L-tryptophanyl-L-prolyl-cysteinamide, cyclic [1–6]-disulfide)]. It was used at concentrations, determined spectrally, that yielded >80%

receptor saturation (15). Synthetic peptide L-histidyl-L-histidyl-L-leucyl-glycyl-glycyl-L-alanyl-L-lysyl-L-glutamyl-L-alanyl-glycyl-L-aspartyl-L-valine (HHLGGAKQAGDV) was prepared and characterized by the Protein Analysis Core Laboratory of the Comprehensive Cancer Center of Wake Forest University; peptide concentrations were determined by amino acid analysis.

**Fibrinogen.** Highly purified human fibrinogen, free of plasminogen and Factor XIII, was purchased from American Diagnostica (Stamford, CT). Following reconstitution in HSCM buffer and extensive dialysis, fibrinogen concentrations were determined spectrally (48).

**Recombinant Fibrinogens.** Normal and  $\gamma\Delta 408$ –411 recombinant fibrinogens were synthesized in CHO cells as described previously (41, 49). Cells were cultured in roller bottles by Biovest International Inc./NCCC (Minneapolis, MN). Serum-free medium containing secreted fibrinogen was harvested periodically; protease inhibitors were added, and the medium was stored at  $-20^\circ\text{C}$  prior to being shipped on dry ice. Recombinant fibrinogen was purified as described previously (41, 49). Briefly, fibrinogen was precipitated from the medium with ammonium sulfate in the presence of a cocktail of protease inhibitors. The precipitate was resuspended in buffer containing 10 mM  $\text{CaCl}_2$  and applied to a Sepharose 4B column coupled with the fibrinogen-specific monoclonal antibody, IF-1. Fibrinogen was eluted from the column with buffer containing 5 mM EDTA, dialyzed against HBS [20 mM HEPES (pH 7.4) and 150 mM NaCl] and 1 mM  $\text{CaCl}_2$  for one exchange, then extensively dialyzed against HBS, and stored at  $-80^\circ\text{C}$ . The integrity of the polypeptide chains and the purity of the recombinant protein were analyzed by SDS–PAGE under reduced and nonreduced conditions.

**Surface Plasmon Resonance Spectroscopy.** Measurements were performed in a Biacore T100 instrument by monitoring the changes in response units (RU) at the biosensor surface (47). Signals from both the reference and sample channels were collected at a rate of 10 Hz. Reagents were maintained at  $25.0 \pm 0.1^\circ\text{C}$  in the sample compartment; data were collected at 37, 25, or  $15^\circ\text{C}$  with control to  $\pm 0.01^\circ\text{C}$  in the analysis chamber.

Purified A4 IgG, specific for the integrin  $\alpha\text{IIb}$  carboxy-terminal segment, was covalently coupled to the sample and reference cells of CM-5 chips to achieve a surface density of 10000–12000 RU, followed by ethanolamine blocking (16). Most experiments used primed integrins, delivered to the sample channel at  $530 \pm 120 \text{ nM}$  ( $n = 16$ ) in HSCM-OG in the presence of a 6-fold molar excess of eptifibatide. In selected experiments, resting integrins at  $370 \pm 170 \text{ nM}$  ( $n = 2$ ) were captured in HSCM-OG. Following the initial capture step, samples were stabilized for 20 min, while HSCM-T buffer flowed over the chip. Note that this step removed the octyl glucoside and priming agent (16). Similar capture levels resulted at  $37^\circ\text{C}$  with primed ( $300 \pm 150 \text{ RU}$ ;  $n = 12$ ) and resting integrins ( $124 \pm 59 \text{ RU}$ ;  $n = 2$ ). Increased levels were obtained with primed receptors at lower temperatures:  $502 \pm 47 \text{ RU}$  ( $n = 2$ ) at  $25^\circ\text{C}$  and  $514 \pm 58 \text{ RU}$  ( $n = 2$ ) at  $15^\circ\text{C}$ . To correct for differences in capture levels, fibrinogen binding signals were normalized by the integrin capture RU for each cycle.

At each temperature, one or two start-up cycles were performed: a midrange fibrinogen concentration (40–50 nM in HSCM-T) was delivered to the sample and reference channels, followed by a two-step regeneration cycle, first with 3 M NaCl and then with pH 3 glycine buffer. Next, during the binding steps, an aliquot of fibrinogen (0–150 nM) was delivered to both flow cells at a rate of 20  $\mu\text{L}/\text{min}$  for 1000 s; dissociation of the

integrin–fibrinogen complexes was then monitored for 1500 s, as HSCM-T buffer flowed over the biosensor surface at a rate of 30  $\mu\text{L}/\text{min}$ . The biosensor was regenerated and equilibrated for 300 s with buffer prior to the next cycle.

Representative RU versus time profiles depicting integrin capture, stabilization, fibrinogen binding (or buffer blank), and regeneration are presented in Figure S1 of the Supporting Information. Note that  $\alpha\text{IIb}\beta 3$  bound rapidly ( $k_{\text{on}} = 1.7 \times 10^4 \text{ L mol}^{-1} \text{ s}^{-1}$ ) to immobilized mAb A4 and then dissociated slowly ( $k_{\text{off}} = 2.5 \times 10^{-5} \text{ s}^{-1}$ ) during the stabilization period. The doubly corrected signals noted earlier account for integrin dissociation effects.

**SPR Kinetic Analyses.** Sensorgram responses, the difference in RU versus time between sample and reference channels at each fibrinogen concentration, were further corrected by subtraction of profiles obtained with a buffer blank. These doubly corrected signals (50) were then fit globally by nonlinear regression (Biacore evaluation software) to a 1:1 binding model (47). The quality of the fits was judged by the residuals as well as the signal-to-noise ratio ( $\langle \text{RU} \rangle / \sqrt{\chi^2}$ ). As described in Table S1 of the Supporting Information, we also explored fitting each data set to a bivalent analyte model, which did not significantly improve the goodness of fit. Table S2 of the Supporting Information shows other analyses that validate the off-rate determinations.

Reasoning that any effects of multisite binding would be minimized at lower integrin capture densities, we conducted a series of fibrinogen binding experiments at input concentrations of primed  $\alpha\text{IIb}\beta 3$  of 251, 125, and 61 nM, yielding integrin capture levels of 276, 147, and 48 RU, respectively. As illustrated in Figure S2 of the Supporting Information, comparable binding and dissociation kinetic profiles resulted at each integrin density. While lower fibrinogen binding levels were observed at lower integrin capture levels, each data set was described well by a 1:1 binding model. The finding that both the forward and reverse rate constants for fibrinogen–integrin interactions were essentially independent of the integrin capture level, over a 6-fold range, indicates that multivalent interactions do not make a significant contribution to complex formation in our system. Hence, we used the 1:1 binding model for all kinetic analyses in this work.

**Solid-Phase Binding Assays.**  $\alpha\text{IIb}\beta 3$  (34  $\mu\text{g}/\text{mL}$ , 150 nM), either resting or primed by incubation with 2  $\mu\text{M}$  eptifibatide for 2 h at 37  $^\circ\text{C}$ , in HSCM-OG was coupled to Pierce Reacti-Bind Amine-Binding Maleic Anhydride 96-well plates and incubated overnight at 4  $^\circ\text{C}$ . Fibrinogen was derivatized with EZ-Link-Sulfo-NHS-biotin (Pierce) in a 2 h reaction in PBS at 0  $^\circ\text{C}$  followed by extensive dialysis at room temperature. The degree of labeling, 7.3 mol of biotin/mol of protein, was determined by difference spectroscopy using an avidin displacement assay (Pierce). Biotinylated fibrinogen samples (0–30 nM) were incubated in integrin-coated or buffer blank wells for 1 h at room temperature, followed by washing and color development steps as previously described (16).

## RESULTS

**Binding of Fibrinogen to Resting and Primed  $\alpha\text{IIb}\beta 3$ .** SPR kinetic data demonstrated that fibrinogen bound rapidly and tightly to primed, but not resting,  $\alpha\text{IIb}\beta 3$  receptors immobilized on a biosensor (Figure 1A). Fitting the data obtained with primed  $\alpha\text{IIb}\beta 3$  and fibrinogen (5–150 nM) to a 1:1 binding model (eq 1) yielded a close correspondence between the data

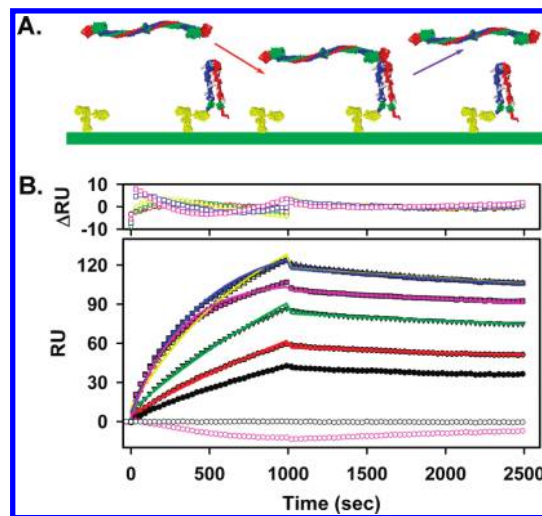
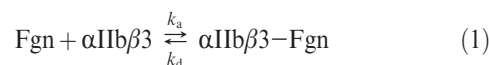


FIGURE 1: Kinetics of binding of fibrinogen to  $\alpha\text{IIb}\beta 3$  determined by surface plasmon resonance. (A) Schematic of integrin immunocapture on a biosensor surface, followed by reversible fibrinogen binding. (B) SPR kinetic traces depicting the time course of concentration-dependent binding of fibrinogen to eptifibatide-primed  $\alpha\text{IIb}\beta 3$ . The following fibrinogen concentrations were used: 5 (black), 10 (red), 20 (green), 50 (yellow), 100 (blue), and 150 nM (pink). The weakened signals at 100 and 150 nM fibrinogen were caused by less efficient integrin capture in the later cycles of this experiment. Solid lines were determined by fitting the data to a 1:1 reversible binding model; residuals are shown in the top panel. The fitting routine also has a term that accounts for the small, sharp drop in RU at the start of the dissociation step. This effect is due to a slight difference in the refractive index in sample vs running buffer. No fibrinogen binding was detected with resting  $\alpha\text{IIb}\beta 3$  [empty symbols for 5 (black) and 150 nM (pink); data from other concentrations omitted for the sake of clarity]. All data were collected at 37  $^\circ\text{C}$ .

(Figure 1B, filled symbols) and fitted lines as well as a narrow distribution of residuals.



This analysis resulted in a  $k_a$  of  $(2.19 \pm 0.01) \times 10^4 \text{ L mol}^{-1} \text{ s}^{-1}$ , a  $k_d$  of  $(7.01 \pm 0.04) \times 10^{-5} \text{ s}^{-1}$ , and a dissociation constant ( $K_d = k_d/k_a$ ) of  $3.20 \times 10^{-9} \text{ M}$  for binding of fibrinogen to primed  $\alpha\text{IIb}\beta 3$  at 37  $^\circ\text{C}$ . In contrast, only negative RU versus time profiles resulted with resting receptors (Figure 1B, empty symbols), indicating no detectable interactions even at 150 nM fibrinogen.

These findings were confirmed with a solid-phase binding assay in which biotinylated fibrinogen (0–30 nM) was incubated with resting or primed  $\alpha\text{IIb}\beta 3$  covalently coupled to the wells of a microtiter plate (16). Fibrinogen exhibited a hyperbolic, saturable binding profile with the primed receptor, characterized by a  $2.0 \pm 0.4 \text{ nM}$  midpoint. In contrast, signals obtained with resting integrins exhibited a shallow, linear dependence on fibrinogen concentration. These data indicate that fibrinogen binds  $\sim 100$ -fold more tightly to primed, compared to resting, integrins (Figure S3 of the Supporting Information).

**Blocking Binding of Fibrinogen to Primed  $\alpha\text{IIb}\beta 3$ .** Next, we investigated the paradox that eptifibatide, the integrin antagonist that we used to prime  $\alpha\text{IIb}\beta 3$  here and in our previous studies with PAC-1(16), also inhibits binding of fibrinogen to its platelet receptors (51). SPR kinetic data demonstrated that delivering fibrinogen (100 nM) in the presence of eptifibatide (10 nM) weakened the binding signal 5-fold compared to a control; 100 nM eptifibatide resulted in near-complete binding inhibition (Figure 2). These data are presented as the ratio of the



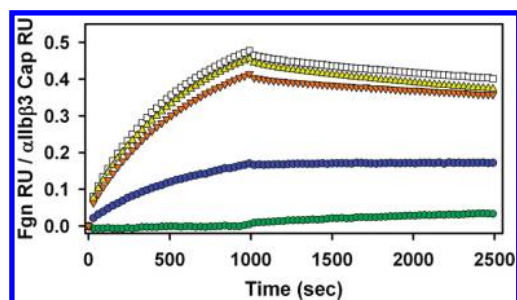


FIGURE 2: Inhibition of binding of fibrinogen to  $\alpha$ IIb $\beta$ 3 by eptifibatide and HHLGGAKQAGDV  $\gamma$ C peptide. To facilitate comparison between experiments, SPR kinetic traces are presented as the ratio of the fibrinogen binding signals to those for  $\alpha$ IIb $\beta$ 3 immunocapture: (empty squares) 100 nM fibrinogen binding control, (yellow triangles) 100 nM fibrinogen and 300 nM  $\gamma$ C peptide, (orange triangles) 100 nM fibrinogen and 3000 nM  $\gamma$ C peptide, (blue circles) 100 nM fibrinogen and 10 nM eptifibatide, and (green circles) 100 nM fibrinogen and 100 nM eptifibatide. All data were collected at 37 °C.

fibrinogen binding RU signal to the  $\alpha$ IIb $\beta$ 3-captured RU signal to facilitate comparison between experiments.

Analysis of the complete data set with a competitive inhibition model demonstrated eptifibatide (10–1000 nM) reduced the level of fibrinogen binding by 50% at a mole ratio of  $0.08 \pm 0.03$  (Figure S4 of the Supporting Information). This result indicates that eptifibatide binds  $\sim 10$ -fold tighter than fibrinogen to  $\alpha$ IIb $\beta$ 3. These findings were confirmed with a solid-phase binding assay that demonstrated that eptifibatide (2  $\mu$ M) reduced the level of fibrinogen binding (0–30 nM) to near-background levels (Figure S4 of the Supporting Information). We conclude that eptifibatide's ability to bind tightly to  $\alpha$ IIb $\beta$ 3 (15), shifting it from a resting to a ligand-competent conformation (16, 52), and then to dissociate rapidly (16) contributes to its ability to both promote and block binding of fibrinogen to  $\alpha$ IIb $\beta$ 3.

Given the importance of the carboxy terminus of fibrinogen's  $\gamma$ -module in promoting interactions with  $\alpha$ IIb $\beta$ 3 (10, 53, 54), we investigated the ability of a synthetic peptide spanning that sequence to block binding of fibrinogen to primed  $\alpha$ IIb $\beta$ 3. SPR kinetic data demonstrated that peptide HHLGGAKQAGDV was a weak inhibitor, reducing the magnitude of the fibrinogen binding signal by  $<10\%$  at 3  $\mu$ M, a 30-fold molar excess (Figure 2 and Figure S4 of the Supporting Information). This observation fits with the findings of Kloczewiak et al. (55), who first developed a series of  $\gamma$ C peptides as platelet-aggregation inhibitors. They reported an  $IC_{50}$  of 28  $\mu$ M (165-fold molar excess) for HHLGGAKQAGDV inhibition of binding of [ $^{125}$ I]-fibrinogen to human platelets; maximal inhibition of platelet aggregation required 60  $\mu$ M peptide (55). Because conformational flexibility could limit this synthetic ligand's effectiveness, we also measured  $\alpha$ IIb $\beta$ 3's interactions with a recombinant fibrinogen variant lacking critical residues in its  $\gamma$ -module.

**Recombinant Fibrinogen Binding to Primed  $\alpha$ IIb $\beta$ 3.** SPR demonstrated that normal recombinant fibrinogen (Figure 3A, filled symbols) bound rapidly and tightly to immunocaptured, eptifibatide-primed  $\alpha$ IIb $\beta$ 3 at 37 °C. Fitting the kinetic data obtained in three experiments with normal rFgn (10, 20, 25, 30, 60, 100, 125, and 150 nM) to a 1:1 binding model (eq 1) yielded the resultant kinetic parameters [ $k_a = (2.19 \pm 0.01) \times 10^4$  L mol $^{-1}$  s $^{-1}$ ,  $k_d = (3.94 \pm 0.01) \times 10^{-5}$  L mol $^{-1}$  s $^{-1}$ , and  $K_d = 1.80 \times 10^{-9}$  M] are comparable to those obtained with highly purified human plasma fibrinogen (Figure 1). In contrast, no binding signals were detected with rFgn  $\gamma\Delta 408$ –411, even at 100 nM (Figure 3A, empty symbols).

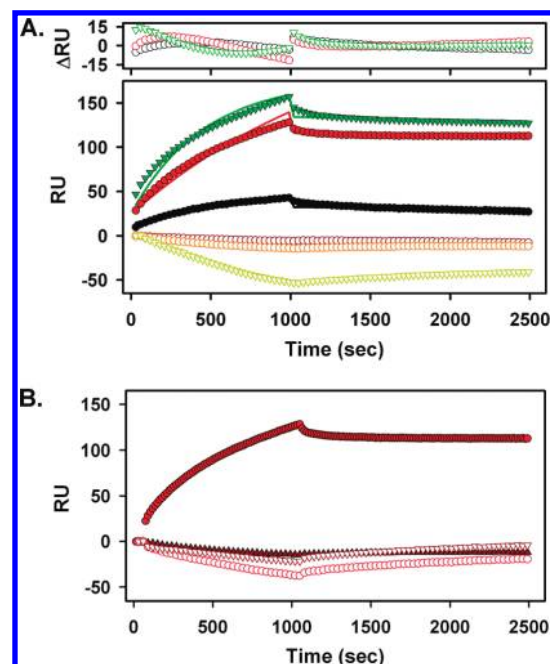


FIGURE 3: Kinetics of binding of recombinant fibrinogen to primed  $\alpha$ IIb $\beta$ 3 determined by surface plasmon resonance. (A) SPR kinetic traces depicting the time course of concentration-dependent binding of normal recombinant fibrinogen (10, 30, and 100 nM) to eptifibatide-primed  $\alpha$ IIb $\beta$ 3 (filled symbols). Solid lines were determined by global fitting of the complete data set (three experiments and eight fibrinogen concentrations) to a 1:1 reversible binding model; residuals are shown in the top panel. No binding was detected with rFgn  $\gamma\Delta 408$ –411 (empty symbols). All data were collected at 37 °C. (B) SPR kinetic traces showing eptifibatide inhibition of binding of recombinant fibrinogen to primed  $\alpha$ IIb $\beta$ 3. Normal recombinant fibrinogen (30 nM, red circles) and eptifibatide (26  $\mu$ M, empty circles). Note the complete inhibition. rFgn  $\gamma\Delta 408$ –411 (30 nM, dark red triangles) and eptifibatide (26  $\mu$ M, empty triangles). Note the similar negative RU traces in both cases.

Excess eptifibatide fully blocked normal rFgn binding, reducing the time-dependent RU traces to the background levels observed with rFgn  $\gamma\Delta 408$ –411 (Figure 3B). Note that excess eptifibatide had little effect on the near-baseline RU signals obtained with this mutant. Taken together, the observations in Figure 3 indicate that both plasma and recombinant fibrinogens use similar mechanisms to bind primed  $\alpha$ IIb $\beta$ 3 with similar specificity.

**Temperature Dependence of  $\alpha$ IIb $\beta$ 3–Fibrinogen Binding.** Measuring the temperature dependence of binding of fibrinogen to primed  $\alpha$ IIb $\beta$ 3 provided additional insights into the mechanisms that regulate these interactions. Figure 4 presents SPR kinetic traces obtained at 37, 25, and 15 °C with plasma fibrinogen; data are presented as the ratio of the fibrinogen-bound to integrin-capture RU signals to facilitate comparisons. Binding specificity was confirmed with blocking experiments performed at 100 nM fibrinogen and 20  $\mu$ M eptifibatide, which reduced the signal below background levels at each temperature.

The solid lines in each panel were obtained by a global fit of data obtained in duplicate experiments to a 1:1 binding model to determine the on and off rate constants and, from them, the dissociation constant at each temperature. In each case, the narrow distribution of residuals confirms the validity of the fits. Data obtained at 37 °C yielded a  $k_a$  of  $(1.90 \pm 0.01) \times 10^4$  L mol $^{-1}$  s $^{-1}$ , a  $k_d$  of  $(8.41 \pm 0.03) \times 10^{-5}$  s $^{-1}$ , and a  $K_d$  of  $4.42 \times 10^{-9}$  mol/L. At 15 °C, the on rate was  $\sim 2$ -fold slower and the off

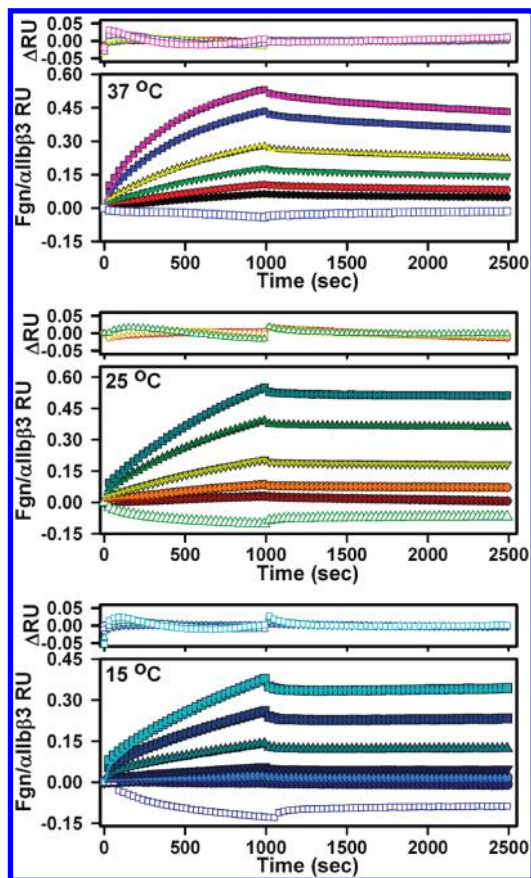


FIGURE 4: Temperature dependence of the kinetics of fibrinogen binding to primed  $\alpha\text{IIb}\beta 3$  determined by surface plasmon resonance. To facilitate comparison between experiments, SPR kinetic traces are presented as the ratio of the fibrinogen binding signals (5, 10, 20, 50, 100, and 150 nM) to those for  $\alpha\text{IIb}\beta 3$  immunocapture. Solid lines were determined by fitting the data in duplicate experiments to a 1:1 reversible binding model; residuals are presented in the top panels. The empty symbols denote the inhibitory effects of excess eptifibatide (26  $\mu\text{M}$ ) on binding of 100 nM fibrinogen.

rate  $\sim 7$ -fold slower, yielding  $\sim 4$ -fold tighter binding at the lower temperature. Intermediate values were obtained at 25  $^{\circ}\text{C}$ .

**Equilibrium and Transition-State Thermodynamic Data for  $\alpha\text{IIb}\beta 3$ –Fibrinogen Binding.** A van't Hoff plot (47, 56) of the temperature dependence of  $K_d$ , determined from the ratio of the reverse and forward rate constants at each temperature, yielded a negative slope and a near-zero intercept (Figure 5A). The resultant equilibrium thermodynamic parameters indicated fibrinogen binding is enthalpy-driven, characterized by a  $\Delta H^{\circ}$  of  $-11.7 \pm 4.4$  kcal/mol and a  $\Delta S^{\circ}$  of  $\sim 0$ . Following Eyring's reaction rate formalism (47, 57), plotting the temperature dependence of the rate constants (Figure 5B) yielded a set of transition-state thermodynamic parameters. This analysis demonstrated that the transition-state free energy barrier ( $\Delta G^{\ddagger} = 11.8 \pm 5.2$  kcal/mol) is dominated by an unfavorable activation entropy ( $\Delta S^{\ddagger} = -28.5 \pm 12.5$  cal  $\text{K}^{-1} \text{mol}^{-1}$ ) while the enthalpic contribution ( $\Delta H^{\ddagger}$ ) approaches 0. These points are summarized in the reaction coordinate diagram presented in Figure 6.

## DISCUSSION

**Integrin Antagonist Priming Mechanisms.**  $\alpha\text{IIb}\beta 3$  normally resides in a quiescent conformation (31, 34, 58) rendered inaccessible to macromolecular ligands by an activation energy barrier ( $\Delta G^{\ddagger} > 10$  kcal/mol) (16). In contrast, pharmaceutical

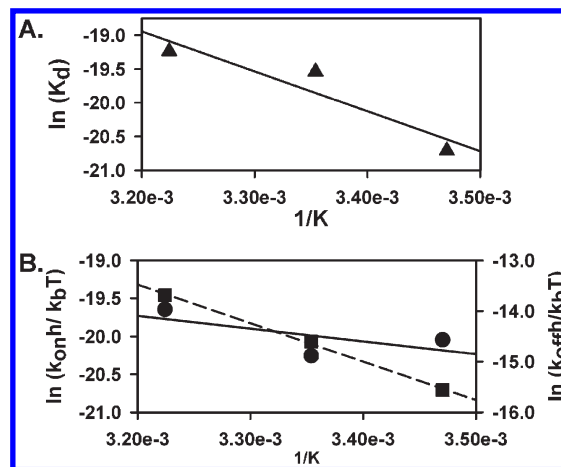


FIGURE 5: Equilibrium and transition-state thermodynamic analyses of binding of fibrinogen to primed  $\alpha\text{IIb}\beta 3$ . (A) van't Hoff analysis of the temperature dependence of the equilibrium dissociation constants for  $\alpha\text{IIb}\beta 3$ –fibrinogen complexes. The solid line was determined by linear regression. Enthalpy ( $\Delta H^{\circ}$ ) and entropy ( $\Delta S^{\circ}$ ) changes for  $\alpha\text{IIb}\beta 3$ –fibrinogen binding were determined from the regression line's slope and intercept, respectively (47). (B) Eyring analysis of the temperature dependence of the forward and reverse rate constants for  $\alpha\text{IIb}\beta 3$ –fibrinogen complexes. Data are presented as the logarithm of the association rate,  $k_a$  data, divided by the kelvin temperature, and scaled by the ratio of Planck's constant,  $h$ , to Boltzmann's constant,  $k_b$ , plotted vs  $1/T$  ( $\bullet$ ). The activation enthalpy ( $\Delta H_a^{\ddagger}$ ) and entropy ( $\Delta S_a^{\ddagger}$ ) were calculated from the slope and intercept, respectively, of the solid line, determined by linear regression, as described previously (47). Analogous procedures for the dissociation rate constant,  $k_d$  ( $\blacksquare$  with dashed line), yielded  $\Delta H_d^{\ddagger}$  and  $\Delta S_d^{\ddagger}$ .

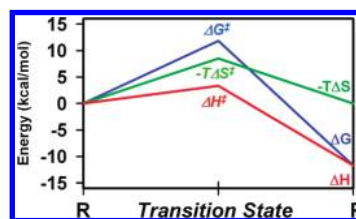


FIGURE 6: Free energy profile for  $\alpha\text{IIb}\beta 3$ –fibrinogen complexes. Changes in free energy, enthalpy, and entropy are depicted along the path from reactants to products. Note that binding requires overcoming an entropy-dominated transition-state barrier before an enthalpy-stabilized receptor–ligand complex is reached.

integrin antagonists readily bind to the resting integrin and shift the equilibrium toward a primed conformer that remains populated at least 90 min post-receptor occupancy (15, 16). In this work, we showed how this conformational hysteresis provides a window for avid fibrinogen binding.

Thanks to recent X-ray diffraction crystallographic structures of integrins, we can consider molecular mechanisms that may explain our observations. Structural data for  $\alpha\text{IIb}\beta 3$ 's resting ectodomain (Protein Data Bank entry 3FCS) (6) as well as complexes with eptifibatide (Protein Data Bank entry 2VDN) (6, 9) and fibrinogen's  $\gamma$ -C peptide (Protein Data Bank entry 2VDO) (10) provide insights into subtle rearrangements that accompany ligand binding at the interface between  $\alpha\text{IIb}$ 's  $\beta$ -propeller and  $\beta 3$ 's I domain. As illustrated in Figure 7, both these ligands occupy similar positions when bound to the  $\alpha\text{IIb}\beta 3$  ectodomain. The overall size of  $\alpha\text{IIb}\beta 3$ 's ligand-binding pocket, measured as the distance between the MIDAS  $\text{Mg}^{2+}$  and the salt-bridging carboxylate anion on  $\alpha\text{IIb}$  D224, was 19.9 Å in the resting ectodomain, 19.5 Å with eptifibatide bound, and 19.7 Å



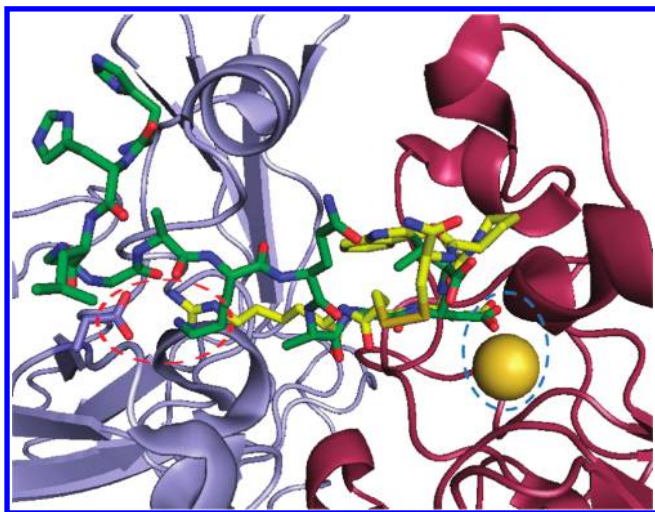


FIGURE 7: Integrin–ligand binding modes. Fibrinogen’s  $\gamma$ C peptide (green backbone) and eptifibatide (yellow backbone) occupy similar positions in  $\alpha$ IIb $\beta$ 3’s ligand-binding crevice.  $\alpha$ IIb and  $\beta$ 3 polypeptides are shown as blue and red ribbons, respectively; highlighted atoms shown in ball-and-stick representation are color-coded as follows: red for oxygen and blue for nitrogen. In both cases, a ligand aspartate forms an electrostatic contact with the  $\beta$ 3 subunit’s MIDAS  $\text{Mg}^{2+}$  (highlighted by the blue-dashed ellipse). Additional stabilization is provided by a tight turn that enables the  $\gamma$ C lysine’s  $\zeta\text{N}^+$  atom to form a salt bridge with a carboxylate anion on  $\alpha$ IIb’s Asp224; the  $\eta\text{N}^+$  atom on eptifibatide’s homoarginine makes a similar contact (highlighted by a red-dashed ellipse). This figure was prepared with Pymol (76) and is based on crystal structure data presented by Springer et al. (10) for complexes formed between  $\alpha$ IIb $\beta$ 3’s ectodomain and fibrinogen’s  $\gamma$ C peptide (Protein Data Bank entry 2VDO) and eptifibatide (Protein Data Bank entry 2VDN).

with HHLGGAKAQGDV bound. Because even the resting receptor’s pocket appears to be sufficiently large to fit the  $\gamma$ -C peptide, whose zwitterions are separated by only 17 Å, we must consider other factors to understand how fibrinogen binding is regulated.

Using the metal ion-dependent adhesion site (MIDAS) as a reference, we find that ligand binding shifts the adjacent  $\text{Ca}^{2+}$  ion in the AdMIDAS site, considered a negative regulator of adhesiveness (59), some 2–3 Å closer to the MIDAS  $\text{Mg}^{2+}$ . Perhaps more importantly, that  $\text{Ca}^{2+}$  moves within  $\sim 4$  Å of the carboxylate anion on  $\beta$ 3 residue D251, a distance that allows electrostatic interactions (60). As Zhu et al. (6) demonstrated, the net increased positive charge on the MIDAS  $\text{Mg}^{2+}$  now favors strong ionic interactions with aspartate carboxylates that reside  $\sim 3$  Å away on both eptifibatide and fibrinogen’s  $\gamma$ -C peptide.

While these conformational changes are likely to be readily reversible, they are linked to larger polypeptide chain rearrangements initiated by downward movement of  $\beta$ 3’s  $\alpha 7$  helix and swing-out of its hybrid domain (9). Allosteric propagation through  $\beta$ 3’s hybrid and PSI domains disrupts contacts with  $\alpha$ IIb’s thigh domain, eventually leading to an extended integrin with a gap between its transmembrane and cytoplasmic domains (11). We propose that the substantial conformational changes that characterize this maximally activated integrin (14) may well account for the metastable, integrin-antagonist primed state that binds fibrinogen (this work) and PAC-1 (16), each with nanomolar affinity.

**Factors Limiting the On and Off Rates of the Fibrinogen– $\alpha$ IIb $\beta$ 3 Complex.** We demonstrated that fibrinogen binds rapidly to eptifibatide-primed  $\alpha$ IIb $\beta$ 3 ( $k_a \sim 2 \times 10^4 \text{ L mol}^{-1} \text{ s}^{-1}$  at 37 °C). However, this process is  $\sim 70$ -fold slower than the initial

step in forming an activated integrin–PAC-1 complex (16), which raises a question. What factors limit fibrinogen binding? Structural data indicate that both macromolecular ligands recognize  $\alpha$ IIb $\beta$ 3 through similar zwitterionic interactions (10, 61). While PAC-1’s RYD sites reside on a loop on the IgM’s Fab domains (61, 62), the integrin targeting sequence at the carboxy terminus of fibrinogen’s  $\gamma$ C module exhibited no discernible electron density in crystal structures of human fibrinogen (63), fragment D-dimer (64), or recombinant fragment D (65). These observations suggest that the  $\gamma$ -chain segment on fibrinogen is highly flexible (63, 66) and possibly intrinsically disordered (10).

In contrast, when bound to the  $\alpha$ IIb $\beta$ 3 ectodomain, synthetic HHLGGAKQAGDV displays a unique structure (10), characterized by a tight turn that positions its lysine’s  $\zeta\text{N}^+$  atom within 3 Å of a carboxylate anion on  $\alpha$ IIb’s Asp224 (Figure 7). The ligand’s aspartate is likewise within 3 Å of the  $\beta$ 3 MIDAS  $\text{Mg}^{2+}$ , providing a key source of stability. Indeed, our studies with rFgn  $\gamma\Delta 408$ –411 clearly confirm that this electrostatic contact is an essential feature of the  $\alpha$ IIb $\beta$ 3–fibrinogen complex. The contrast between the tightly structured  $\gamma$ C peptide– $\alpha$ IIb $\beta$ 3 ectodomain complex and fibrinogen’s flexible  $\gamma$ -chain carboxy terminus may explain our observation that the activation free energy barrier between reactants and products is dominated by an unfavorable entropy term (Figure 6). We propose that the conformational entropy cost of transition-state formation strongly contributes to the relatively slow rate of integrin–fibrinogen binding.

Once bound, fibrinogen dissociates quite slowly from the primed  $\alpha$ IIb $\beta$ 3 receptor, exhibiting a decay time of  $\sim 200$  min at 37 °C, some 70-fold slower than that of eptifibatide (16). On the basis of our experience studying  $\alpha$ IIb $\beta$ 3’s interactions with pentameric PAC-1 (16), we recognized that these rather slow off rates might be due to multivalent interactions with fibrinogen, a covalent ( $\text{A}\alpha\text{B}\beta\gamma$ )<sub>2</sub> homodimer with an integrin targeting sequence on each of its distal  $\gamma$ -modules. In their classic study of the interactions between human growth hormone and its receptor’s extracellular binding domain, Cunningham and Wells (67) demonstrated by SPR that blocking formation of dimeric receptor–ligand complexes increased the dissociation rate constant from  $< 10^{-5}$  to  $\sim 4 \times 10^{-4} \text{ s}^{-1}$ . Similarly, Duan et al. (68) reported minimal dissociation for a pentameric monobody bound to the  $\alpha\text{v}\beta$  integrin, while a single-domain construct dissociated at least 100-fold faster. However, our fibrinogen binding kinetic data were not influenced by the integrin capture level (Figure S2 of the Supporting Information), and fitting them to a bivalent analyte model yielded no significant improvement in the goodness of fit (Table S1 of the Supporting Information); therefore, we conclude that fibrinogen binding to multiple immobilized integrins did not make a significant contribution to our findings.

Alternatively, several lines of evidence indicate that while fibrinogen shares a zwitterionic binding motif with eptifibatide (10), its macromolecular multidomain structure provides additional binding sites that may stabilize its complex with  $\alpha$ IIb $\beta$ 3. In addition to fibrinogen’s primary integrin-recognition motif,  $\gamma 400$ –411, auxiliary integrin binding sites have been localized to  $\gamma 316$ –322 (42–44) and  $\gamma 370$ –381 (45, 46). Likewise, mutagenesis studies have identified a cluster of residues critical to fibrinogen binding in the cap subdomain of  $\alpha$ IIb’s  $\beta$ -propeller region (69, 70) and on  $\beta$ 3’s specificity-determining loop (9, 71).

The extensive area capable of encompassing these putative contacts between  $\alpha$ IIb $\beta$ 3’s ectodomain and fibrinogen’s  $\gamma$ C module may well be responsible for the longevity of the integrin–fibrinogen complex. This concept is supported by our observation

(Figure S5 of the Supporting Information) of relatively slow dissociation rates, even for  $\alpha\text{IIb}\beta 3$ 's interactions with echistatin, a 49-residue disintegrin with a single RGD site (47). Echistatin's nine-residue carboxy-terminal segment may provide additional contacts that contribute to the stability of its complex with  $\alpha\text{IIb}\beta 3$ , and similar mechanisms may stabilize fibrinogen binding. Indeed, we only observed rapid dissociation of  $\alpha\text{IIb}\beta 3$  from cHarGD, a monovalent cyclic peptide integrin antagonist (72).

**Physiological Regulation of Integrin Activation.** We recognize the challenges in extrapolating from a well-characterized receptor–ligand system to an environment of densely packed  $\alpha\text{IIb}\beta 3$  receptors with their extracellular domains protruding from a platelet surface, linked through transmembrane segments to distant cytoplasmic domains. Recent advances in cell biology, biochemistry, biophysics, and structural biology have demonstrated how integrin-associated proteins, especially talin and kindlins, control the receptor's activation state through interactions with  $\beta 3$ 's cytodomain, the phospholipid bilayer, and the actin cytoskeleton (6, 7, 73, 74). Our model system is not designed to address the multiplicity of these protein–protein and protein–lipid interactions. Conversely, because cytodomain separation has emerged as a hallmark of integrin activation (6, 7, 75), our immunocapture of  $\alpha\text{IIb}\beta 3$  through its  $\alpha\text{IIb}$  carboxy terminus may stabilize the receptor's primed conformation, replicating mechanisms that regulate binding to its primary physiological ligand, fibrinogen.

## CONCLUSIONS

We demonstrated that fibrinogen's interactions with the  $\alpha\text{IIb}\beta 3$  integrin are dynamically regulated by priming-induced conformational changes in the receptor's ectodomain. Our studies with recombinant fibrinogen, coupled with structural insights, support the postulate that the stability of the integrin–fibrinogen complex depends on electrostatic interactions between an aspartate residue on the carboxy terminus of fibrinogen's  $\gamma$ -module and the  $\beta 3$  subunit's MIDAS  $\text{Mg}^{2+}$  ion. Our equilibrium and transition-state thermodynamic analyses suggest that locking the initially flexible integrin targeting segment into a binding-competent conformation requires overcoming a substantial entropy barrier. Only then can the enthalpy-favorable, long-lived integrin–fibrinogen complex be assembled. We speculate that kinetics and thermodynamics interact to localize the initiating events in hemostasis to vascular injury sites.

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## SUPPORTING INFORMATION AVAILABLE

Results of fitting each integrin–fibrinogen binding data set to both a single-site and a bivalent analyte model (Table S1), procedures used to validate the off rate determinations (Table S2), SPR time courses of integrin capture by mAb A4, stabilization, fibrinogen binding, dissociation, and regeneration (Figure S1),

SPR fibrinogen binding profiles obtained as a function of the primed integrin capture level (Figure S2), data from solid-phase assays measuring binding of biotin-labeled fibrinogen to resting, primed, and primed and eptifibatide-blocked  $\alpha\text{IIb}\beta 3$  (Figure S3), SPR data examining concentration-dependent inhibition of binding of fibrinogen to immunocaptured, primed  $\alpha\text{IIb}\beta 3$  by eptifibatide and synthetic peptide HHLGGAKQAGDV (Figure S4), and SPR kinetics and binding modes for fibrinogen– $\alpha\text{IIb}\beta 3$ , PAC-1– $\alpha\text{IIb}\beta 3$ ,  $\alpha\text{IIb}\beta 3$ –echistatin, and  $\alpha\text{IIb}\beta 3$ –cHarGD complexes (Figure S5). This material is available free of charge via the Internet at <http://pubs.acs.org>.

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